

Sensor-Based Rehabilitation with Motor Recovery in Post-Stroke Home Programs: Survey Analysis

Juliana Méndez Castro^{1*}, Zi Gu², Hui Gong²

¹ School of Medicine, Universidad de Los Andes, Bogotá, Bogota D.C., Colombia

² Department of Occupational and Environmental Health, School of Public Health, Central South University, Changsha, Hunan, China

Corresponding author: juliana.m.castro@gmail.com

Abstract

Stroke remains a leading cause of long term adult disability worldwide, necessitating extensive and prolonged rehabilitation to restore motor function and improve the quality of life for survivors. As healthcare systems face increasing burdens and resource constraints, traditional in-clinic therapy is frequently insufficient to provide the intensive, high dosage practice required for optimal neuroplasticity. Consequently, sensor based rehabilitation in home programs has emerged as a critical paradigm shift in post stroke care. This paper presents a comprehensive survey analysis of current sensor technologies, including inertial measurement units, surface electromyography, and force sensors, detailing their application in monitoring and facilitating motor recovery outside clinical settings. We analyze the underlying mechanisms of motor recovery, emphasizing how high fidelity sensorimotor feedback promotes neuroplasticity. Furthermore, we examine the system architectures, gamification strategies, and usability factors that define successful home based interventions. By synthesizing clinical outcomes related to both upper and lower extremity recovery, this survey highlights the efficacy of continuous, objective kinematic monitoring. Finally, we discuss existing technical and compliance challenges, offering future perspectives on the integration of wearable sensors into personalized, long term stroke rehabilitation regimens.

Keywords: *Stroke Rehabilitation; Wearable Sensors; Motor Recovery; Home Based Therapy; Sensor-Based Rehabilitation*

1. Introduction

1.1 Background on Stroke and Motor Impairments

Stroke is a profound global health crisis, representing a major cause of mortality and chronic disability across diverse populations. When a cerebrovascular accident occurs, the interruption of blood supply to the brain results in the rapid death of neural tissue, leading to a cascade of neurological deficits. Among the most prevalent and debilitating of these deficits are motor impairments, which affect a significant majority of stroke survivors. Hemiparesis, characterized by weakness or partial paralysis on one side of the body, fundamentally alters a patient's ability to perform routine activities. Additionally, patients frequently experience spasticity, loss of selective motor control, and impaired interlimb coordination. The resultant limitations in mobility and fine motor skills severely diminish independence and overall quality of life. Traditional rehabilitation models rely heavily on face to face interactions between patients and therapists within acute and subacute clinical settings. During these sessions, physical and occupational therapists guide patients through repetitive task specific

movements designed to stimulate neural reorganization. However, the constraints of conventional healthcare systems, including limited personnel, geographical barriers, and insurance restrictions, often mean that patients receive a fraction of the therapy dosage required to maximize their physiological recovery potential. Empirical evidence indicates that high intensity, repetitive, and task oriented training is essential for functional restitution [1]. Consequently, the gap between the requisite amount of therapy and the amount practically delivered in clinic environments has prompted researchers and clinicians to explore alternative paradigms that extend therapeutic interventions beyond the hospital walls.

1.2 The Shift Toward Home Based Rehabilitation

The transition from clinic based to home based rehabilitation represents a necessary evolution in chronic stroke management. Following discharge from acute care, patients often experience a plateau in their recovery trajectory, largely due to a precipitous drop in therapeutic engagement. Home based programs aim to bridge this gap by empowering patients to continue their rehabilitation in a familiar environment. This approach not only alleviates the logistical and financial burdens associated with frequent clinic visits but also aligns with the principles of motor learning, which emphasize the importance of practicing skills in the context of daily living. Historically, home exercise programs relied on printed manuals or verbal instructions, which suffered from notoriously low compliance rates and a lack of objective oversight. Without a therapist present to provide immediate feedback and correct compensatory movement patterns, patients risked ingraining maladaptive habits or abandoning the regimen altogether. The advent of microelectronics and wearable technology has revolutionized this landscape [2]. By integrating miniaturized sensors into clothing, wristbands, or standalone devices, continuous and objective measurement of human movement is now feasible outside the laboratory. Sensor based home rehabilitation systems offer a dual benefit: they provide patients with real time feedback to guide their exercises and furnish clinicians with longitudinal, quantitative data regarding patient adherence and progress. This paradigm shift enables a continuum of care where therapy is integrated seamlessly into daily routines, fostering sustained engagement and theoretically superior motor recovery outcomes.

1.3 Scope and Objectives of the Survey

This paper provides a systematic and comprehensive survey of the current state of sensor based rehabilitation technologies specifically applied to post stroke home programs. The primary objective is to critically evaluate how various sensor modalities capture kinematic and physiological data to facilitate motor recovery. By analyzing the intersection of wearable technology, neuroplasticity, and human computer interaction, this survey aims to elucidate the mechanisms by which sensorimotor feedback enhances therapeutic outcomes in unsupervised settings. We will explore the technical architectures of these systems, including data processing and transmission methodologies, alongside user engagement strategies such as gamification. Furthermore, this paper synthesizes empirical evidence regarding clinical efficacy, focusing on both upper extremity dexterity and lower extremity mobility. A secondary objective is to identify and discuss the persistent challenges hindering widespread clinical adoption, including technical limitations, data privacy concerns, and usability barriers for the elderly stroke demographic. Through this comprehensive analysis, we aim to provide a foundational reference for biomedical engineers, clinical researchers, and healthcare practitioners striving to optimize remote rehabilitation strategies [3].

2. Sensor Modalities in Stroke Rehabilitation

2.1 Inertial Measurement Units and Kinematic Tracking

Inertial measurement units represent the cornerstone of modern wearable movement analysis. These compact electronic devices typically integrate triaxial accelerometers, gyroscopes, and occasionally magnetometers to provide comprehensive data on the orientation and acceleration of the body segment to which they are attached. In the context of post stroke home rehabilitation, inertial measurement units are predominantly utilized to capture the kinematics of the upper and lower extremities. By placing these sensors on strategic anatomical landmarks, such as the wrist, forearm, upper arm, or trunk, systems can reconstruct complex multi joint movements in three dimensional space. Accelerometers measure linear acceleration, including the constant force of gravity, which allows for the estimation of tilt and posture. Gyroscopes measure angular velocity, providing crucial information about the rotation of limbs during dynamic tasks. Sensor fusion algorithms, commonly employing Kalman filters or complementary filters, are utilized to combine data from these constituent sensors, mitigating the inherent drift of gyroscopes and the noise susceptibility of accelerometers. This synergistic data processing yields accurate representations of joint angles, range of motion, and movement smoothness. For stroke survivors, these metrics are vital. Clinicians can remotely monitor whether a patient is achieving the target range of motion during a reaching task or if they are improperly relying on trunk compensation. The unobtrusive nature of inertial measurement units makes them ideal for prolonged home use, allowing for the continuous capture of movement quality during both prescribed exercises and spontaneous activities of daily living [4].

Table 1: Comparison of common sensor modalities used in post stroke home programs

Sensor Modality	Primary Measurement	Key Advantages for Home Use	Common Limitations
Inertial Measurement Units	Linear acceleration and angular velocity	Lightweight, unobtrusive, highly accurate kinematic tracking	Susceptible to drift over time, requires complex calibration algorithms
Surface Electromyography	Muscle electrical activation potentials	Direct measurement of neuromuscular effort and fatigue	Sensitive to skin impedance and electrode placement, signal noise
Force and Pressure Sensors	Mechanical stress and weight distribution	Excellent for gait asymmetry analysis and grasp force measurement	Often confined to specific objects like insoles or smart cups

2.2 Electromyography and Muscle Activity Monitoring

While inertial sensors capture the resultant physical movement, surface electromyography provides a window into the underlying neuromuscular commands generating those movements. Following a stroke, the neural pathways descending from the motor cortex are compromised, leading to disrupted muscle activation patterns. Patients frequently exhibit delayed muscle onset, co-contraction of antagonistic muscle groups, and overall reduced motor unit recruitment. Surface electromyography involves placing non invasive electrodes on the skin overlying specific muscles to record the electrical activity associated with muscle contraction. In home rehabilitation platforms, electromyography serves as a powerful biofeedback mechanism. For instance, a patient attempting to extend their wrist may lack the strength to produce visible movement. However, an electromyography sensor can detect the faint electrical signals indicating an active attempt to contract the extensor muscles. By translating this microscopic electrical activity into macroscopic visual or auditory feedback, the system rewards the patient's neurological effort, reinforcing the neural pathways even in the absence of overt joint rotation [5]. Furthermore, multi channel electromyography can be utilized to identify and discourage maladaptive co-contractions, such as the simultaneous firing of the biceps and triceps, which often impedes smooth reaching motions. Modern advancements have led to the development of wireless, dry electrode electromyography sleeves that eliminate the need for conductive gels and precise anatomical placement, significantly lowering the barrier to entry for independent use by stroke survivors in their homes.

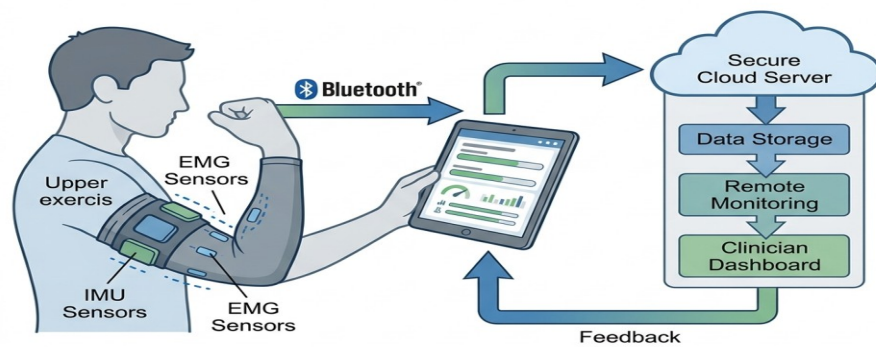


Figure 1: System architecture of a multi

2.3 Force and Pressure Sensors in Activities of Daily Living

Force and pressure sensors add a critical contextual dimension to home based rehabilitation monitoring by quantifying the physical interaction between the patient and their environment. These sensors utilize various technologies, such as piezoresistive materials, capacitive arrays, or strain gauges, to measure the mechanical stress applied to a surface. In lower extremity rehabilitation, pressure sensitive insoles are extensively employed to analyze gait parameters. Hemiparetic stroke survivors often exhibit highly asymmetrical gait patterns, placing disproportionate weight on their non paretic limb to compensate for weakness and balance deficits. Smart insoles continuously map plantar pressure distribution throughout the gait cycle, providing precise metrics on stance time, swing time, and weight bearing symmetry [6]. This data is crucial for preventing long term joint damage and improving walking efficiency. In upper extremity rehabilitation, force sensors are frequently integrated into instrumented objects or smart gloves. Grasping and manipulating objects are fundamental activities of daily living that require intricate coordination and force modulation. Stroke patients may apply excessive grip force due to impaired tactile feedback or insufficient force due to motor weakness. Sensors embedded in smart cups or therapeutic manipulanda can quantify grip strength, pinch force, and the temporal dynamics of object manipulation. This objective quantification of interaction forces provides a highly granular view of fine motor recovery, enabling home systems to adapt the difficulty of grasping tasks based on the patient's real time capabilities.

3. Mechanisms of Motor Recovery and Neuroplasticity

3.1 Principles of Sensorimotor Feedback

The human brain is remarkably adaptable, possessing the intrinsic capacity to reorganize its structure and function in response to experience, learning, and injury. This phenomenon, known as neuroplasticity, is the biological foundation of post stroke motor recovery. The primary mechanism driving this neural reorganization is use dependent plasticity, formulated on the principle that neurons that fire together, wire together. However, mere repetition of movement is insufficient to induce optimal plastic changes. The quality, intensity, and context of the movement are equally critical. Sensor based rehabilitation systems capitalize on these principles by providing immediate, high fidelity sensorimotor feedback. When a patient attempts a movement, the sensory pathways transmit proprioceptive and exteroceptive information back to the central nervous system, creating a closed

control loop. Stroke disrupts this intrinsic feedback mechanism, leaving patients unaware of their movement errors. Wearable sensors bridge this sensory gap by providing extrinsic feedback. For example, if an inertial measurement unit detects improper shoulder elevation during a reaching task, the system can instantly alert the user through an auditory cue or a visual correction on a screen. This real time error augmentation allows the nervous system to recalibrate motor commands iteratively. The immediacy of sensor based feedback strengthens the associative mapping between the intended motor command and the actual kinematic execution, thereby accelerating the consolidation of new, healthy neural connections [7].

Table 2: Mapping of sensor data metrics to standard clinical assessment scales

Clinical Assessment Scale	Target Functional Domain	Corresponding Sensor Derived Metrics
Fugl-Meyer Assessment	Upper extremity motor impairment	Range of motion, movement smoothness (jerk), reaching speed
Wolf Motor Function Test	Time and quality of task execution	Trajectory efficiency, grasping force, task completion duration
Berg Balance Scale	Postural control and stability	Center of pressure displacement, trunk sway velocity, step width

3.2 Quantification of Recovery Metrics

The traditional evaluation of motor recovery relies on standardized clinical scales administered by trained professionals. While these scales are validated and widely accepted, they are inherently subjective, prone to ceiling or floor effects, and only provide a snapshot of the patient's capability at a specific moment in the clinic. Sensor based home programs introduce the paradigm of continuous, objective quantification of recovery metrics. By leveraging sophisticated algorithms, raw sensor data is transformed into clinically meaningful parameters. One of the most frequently analyzed metrics is movement smoothness, often quantified by calculating the spectral arc length or the normalized jerk of a kinematic trajectory [8]. Stroke survivors typically exhibit segmented, jerky movements as they rely on discrete submovements rather than a single fluid motor plan. As neuroplasticity occurs and motor control improves, sensor data will reflect a measurable decrease in movement jerkiness. Another critical metric is the active range of motion, which can be continuously monitored during daily activities to ensure the patient is transferring gains made during active exercise into real world functionality. Furthermore, sensors enable the tracking of usage ratios between the paretic and non paretic limbs. Learned non use is a common phenomenon where patients disproportionately rely on their healthy limb, severely hindering the recovery of the affected side. Wearable devices can passively track upper limb activity throughout the day, providing precise data on arm use asymmetry. This high resolution, longitudinal data stream not only empowers patients with visual evidence of their progress but also allows clinicians to make data driven decisions regarding treatment progression and intervention adjustments.

4. Analysis of Current Home Based Systems and Methodologies

4.1 System Architecture and Data Transmission

The architecture of sensor based home rehabilitation systems is designed to seamlessly acquire, process, and transmit physiological data from the patient's residence to the clinical oversight team. A typical system comprises three distinct layers: the body area network, the local edge processing unit, and the cloud infrastructure. The body area network consists of the distributed wearable sensors, such as inertial measurement units and electromyography nodes, positioned on the patient. These devices must be highly energy efficient to support extended monitoring periods without frequent recharging. Data from these sensors is typically transmitted via low power wireless protocols, such as Bluetooth Low Energy, to a local edge device situated within the home [9]. The edge device, often a dedicated tablet or a smartphone, plays a pivotal role in the system architecture. It serves as the primary user

interface, presenting exercise instructions and real time biofeedback. Moreover, the edge device performs preliminary data processing, filtering raw signals, and computing immediate kinematic metrics to minimize latency in the feedback loop. This local processing is crucial for applications requiring instantaneous responses, such as interactive gaming. Finally, the processed data, along with summary statistics of session duration and task performance, is securely transmitted over the internet to a centralized cloud server. The cloud infrastructure facilitates long term data storage, advanced longitudinal analytics, and provides an accessible dashboard for healthcare professionals to review patient progress asynchronously. This distributed architecture ensures that the system is both responsive to the patient's immediate needs and robust enough for comprehensive clinical monitoring.

4.2 User Engagement and Gamification Strategies

One of the most significant hurdles in post stroke home programs is maintaining long term patient adherence. Rehabilitation exercises are inherently repetitive, arduous, and frequently frustrating for individuals grappling with severe motor deficits. To combat attrition, contemporary sensor based systems heavily integrate gamification strategies to transform tedious exercises into engaging, purpose driven activities. Gamification involves applying game design elements, such as scoring systems, challenges, and immersive narratives, to non game contexts. By coupling the kinematic data derived from wearable sensors with virtual environments, systems create interactive rehabilitation games [10]. For example, a patient's wrist extension, measured by an inertial sensor, might control the altitude of an airplane in a video game, while grasping force, measured by a smart glove, might control the airplane's speed. This mapping of physical movement to virtual outcomes provides intrinsic motivation, shifting the patient's focus away from their physical limitations and toward achieving the game's objectives. Furthermore, gamified systems implement dynamic difficulty adjustment algorithms. These algorithms continuously analyze the patient's sensor data in real time to assess their current capability and fatigue levels. If a patient easily completes a reaching task, the game automatically increases the required range of motion or introduces time constraints to maintain an optimal level of challenge. Conversely, if the patient struggles, the system lowers the difficulty to prevent frustration and demoralization. This tailored, adaptive approach ensures that the therapy remains engaging and optimally therapeutic, significantly enhancing long term compliance rates compared to conventional home exercise programs.

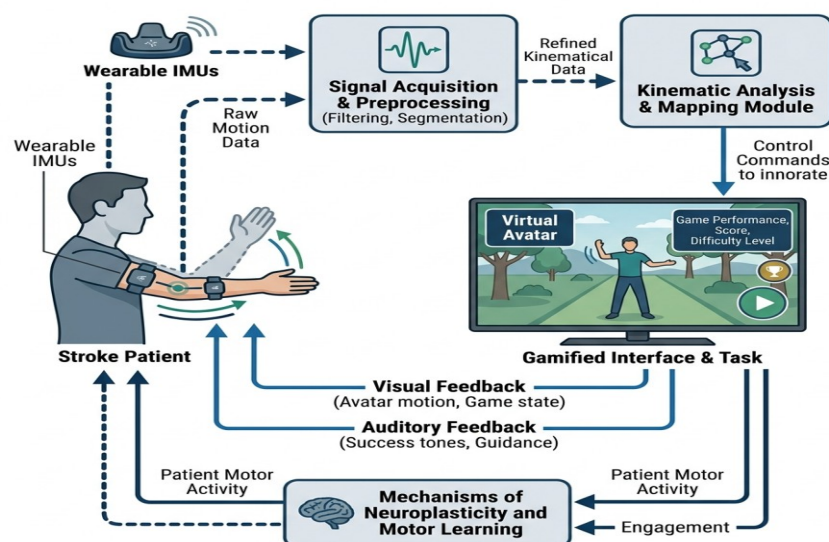


Figure 2: Data flow and feedback loop in gamified sensor

4.3 Patient Compliance and Usability Factors

The technical sophistication of a sensor based system is rendered obsolete if the end user is unable or unwilling to use it. Consequently, usability and patient compliance are critical areas of focus in home rehabilitation design. The target demographic for these systems predominantly consists of elderly individuals who may possess limited technological literacy and may concurrently suffer from cognitive or visual impairments resulting from their stroke. Therefore, user interfaces must be intuitively designed, featuring high contrast visuals, large interactive elements, and clear, unambiguous instructions. The physical design of the sensors themselves is equally paramount [11]. Devices must be lightweight, constructed from hypoallergenic materials, and easy to don and doff independently using only the non paretic hand. Complex calibration procedures or intricate wire management can present insurmountable barriers to daily use. Researchers are increasingly emphasizing participatory design methodologies, involving stroke survivors and therapists in all stages of the development process to identify and mitigate usability pain points early on. Patient compliance is further augmented by features that foster a sense of connection and accountability. Systems that integrate asynchronous messaging or periodic video check ins with a therapist help alleviate the isolation often experienced during home based therapy. When patients understand that their data is actively being reviewed and that their efforts are recognized by their healthcare providers, their motivation to adhere to the prescribed regimen is significantly strengthened.

5. Clinical Outcomes and Efficacy Results

5.1 Upper Extremity Functional Recovery

The efficacy of sensor based home programs in promoting upper extremity recovery has been the subject of extensive empirical investigation. Deficits in the arm and hand are notoriously resistant to treatment, often persisting long after gait has been restored. Studies utilizing wearable inertial measurement units and electromyography have consistently demonstrated that patients engaging in sensor augmented home therapy achieve clinical outcomes that are non inferior, and frequently superior, to conventional unsupervised home programs [12]. The primary driver of these improvements is the substantial increase in therapy dosage facilitated by technology. Patients can comfortably perform hundreds of task specific repetitions daily, guided by precise kinematic feedback. Clinical trials frequently utilize the Fugl-Meyer Assessment for Upper Extremity to quantify recovery. Research indicates that patients utilizing gamified, sensor based systems show significant increases in their Fugl-Meyer scores, reflecting improvements in joint individuation, synergistic movement patterns, and overall motor control. Beyond standardized scales, continuous sensor data provides evidence of qualitative improvements in movement execution. Longitudinal analyses reveal statistically significant reductions in movement trajectory variability and notable increases in peak velocity during reaching tasks. Furthermore, smart glove systems equipped with force sensors have proven highly effective in restoring fine motor dexterity. By practicing object manipulation tasks with real time force feedback, patients demonstrate enhanced ability to modulate grip strength, reducing instances of object dropping or crushing. These functional gains directly translate to an increased ability to perform activities of daily living independently.

Table 3: Summary of clinical efficacy domains in recent sensor-based intervention surveys

Clinical Efficacy Domain	Primary Assessment Method	Observed Impact of Sensor Intervention
Gross Motor Function (Arm)	Reaching kinematics, Fugl-Meyer	Significant improvement in trajectory smoothness and movement speed
Fine Motor Control (Hand)	Instrumented grasping, Box and Blocks	Enhanced precision pinch, better force modulation during object manipulation

Clinical Efficacy Domain	Primary Assessment Method	Observed Impact of Sensor Intervention
Ambulatory Stability (Gait)	Spatiotemporal gait analysis, Timed Up and Go	Increased step symmetry, reduction in compensatory pelvic tilt

5.2 Gait and Lower Extremity Improvements

Lower extremity rehabilitation focuses primarily on restoring safe, efficient, and independent ambulation. Gait impairments following a stroke significantly elevate the risk of falls, leading to further injury and a fear of movement that severely restricts community participation. Sensor based home systems targeting the lower extremities typically deploy inertial sensors on the shanks and thighs, often complemented by pressure sensing insoles. This multi sensor approach allows for a comprehensive biomechanical analysis of the gait cycle in a naturalistic home environment. Clinical outcomes derived from these interventions show marked improvements in spatiotemporal gait parameters [13]. Through targeted auditory or haptic feedback delivered during walking exercises, patients are trained to correct gait asymmetries. For example, if the sensor system detects an abnormally short stance phase on the paretic limb, it can provide rhythmic auditory cueing to encourage equal weight bearing and a more symmetric step length. Over time, this feedback driven training results in a clinically significant increase in walking velocity and a reduction in gait variability. Moreover, continuous monitoring of ambulatory activity provides insights into a patient's overall mobility levels throughout the day. Studies indicate that patients utilizing lower extremity sensor systems demonstrate increased daily step counts and improved scores on clinical mobility assessments such as the Timed Up and Go test. The ability to monitor balance metrics, such as sway velocity and center of mass displacement during transitional movements like standing up from a chair, further contributes to a comprehensive fall prevention strategy, enhancing both physical safety and patient confidence.

6. Conclusion and Future Perspectives

6.1 Technical and Data Security Challenges

Despite the profound potential of sensor based home rehabilitation, several substantial challenges must be addressed to facilitate broad clinical integration. From a technical standpoint, the reliability and accuracy of kinematic data over prolonged, unsupervised periods remain a concern. Wearable sensors, particularly inertial measurement units, are susceptible to signal drift and require sophisticated, robust calibration algorithms that do not burden the user. The physical robustness of the hardware must also withstand the rigors of daily use, sweat exposure, and frequent cleaning. Battery technology poses another limitation; high frequency continuous data sampling rapidly depletes power, necessitating a delicate balance between data resolution and device longevity. Furthermore, the massive volume of high fidelity physiological data generated by these systems introduces critical data security and privacy challenges [14]. Transmitting sensitive health information across domestic Wi-Fi networks and storing it on cloud servers mandates rigorous encryption protocols and compliance with stringent international healthcare data regulations. Patients must be assured that their movement data cannot be intercepted, manipulated, or utilized without explicit consent. Addressing these data governance issues is paramount to building trust among stroke survivors and healthcare institutions.

6.2 Conclusion

This survey has comprehensively analyzed the paradigm of sensor based rehabilitation within post stroke home programs. The integration of wearable modalities, including inertial measurement units, surface electromyography, and force sensors, provides an unprecedented capacity to objectively monitor and quantify human movement outside the traditional clinic. By leveraging the principles of neuroplasticity through high fidelity, real time sensorimotor feedback, these systems address the

critical need for intensive, high dosage therapy in chronic stroke management. The architectural design of home platforms, coupled with sophisticated gamification strategies, effectively mitigates patient attrition by transforming arduous exercises into engaging, purpose driven tasks. Clinical evidence robustly supports the efficacy of these technologies in promoting significant functional gains in both upper extremity dexterity and lower extremity ambulatory capacity. However, overcoming existing barriers related to usability, technical robustness, and data security is essential for the future of remote therapeutics. As miniaturization advances and machine learning algorithms become more adept at interpreting complex physiological signals, sensor based systems will increasingly offer highly personalized, adaptive, and autonomous rehabilitation regimens. Ultimately, the continued evolution and refinement of these technologies hold the promise of democratizing access to high quality, continuous stroke care, fundamentally improving long term recovery trajectories and maximizing the independence of stroke survivors worldwide.

References

1. Foroushani, F.T.; Dzobo, K.; Khumalo, N.P.; Mora, V.Z.; de Mezerville, R.; Bayat, A. Advances in Surface Modifications of the Silicone Breast Implant and Impact on Its Biocompatibility and Biointegration. *Biomater. Res.* 2022, 26, 80.
2. Maxwell, G.P.; Gabriel, A. The Evolution of Breast Implants. *Clin. Plast. Surg.* 2009, 36, 1–13.
3. Cevik, J.; Hunter-Smith, D.J.; Rozen, W.M. Current Advances in Breast Reconstruction. *J. Clin. Med.* 2022, 11, 3328.
4. Lv, X.; Xiang, C.; Zheng, Y.; Xu, S.-F.; Zhou, W.-X.; Lv, X.-L. A Review: Recent Advances in the Application of 3D Printing Biomaterials in Breast Reconstruction Research. *Eur. J. Plast. Surg.* 2024, 47, 38.
5. Magill, L.J.; Tanska, A.; Keshtgar, M.; Mosahebi, A.; Jell, G. Mechanical and Surface Chemical Analysis of Retrieved Breast Implants from a Single Centre. *J. Mech. Behav. Biomed. Mater.* 2019, 91, 24–31.
6. Castner, D.G.; Ratner, B.D. Biomedical Surface Science: Foundations to Frontiers. *Surf. Sci.* 2002, 500, 28–60.
7. Wallach, S.G. Maximizing the Use of the Abdominoplasty Incision. *Plast. Reconstr. Surg.* 2004, 113, 411–417.
8. Geurts, L.S.; Cooke, J.R.H.; van Bergen, R.S.; Jehee, J.F.M. Subjective confidence reflects representation of Bayesian probability in cortex. *Nat. Hum. Behav.* 2022, 6, 294–305.
9. Tavakoli, S.; Nemati, S.; Kharaziha, M.; Akbari-Alavijeh, S. Embedding CuO Nanoparticles in PDMS-SiO₂ Coating to Improve Antibacterial Characteristic and Corrosion Resistance. *Colloid Interface Sci. Commun.* 2019, 28, 20–28.
10. Maxwell, G.P.; Gabriel, A. Breast Implant Design. *Gland Surg.* 2017, 6, 148–153.
11. Prasad, K.; Rifai, A.; Recek, N.; Schuessler, D.; Levchenko, I.; Murdock, A.; Mozetič, M.; Fox, K.; Alexander, K. Nanocarbon-Polymer Composites for Next-Generation Breast Implant Materials. *ACS Appl. Mater. Interfaces* 2024, 16, 50251–50266.
12. Mayo, D.; Hand, D. Statistical significance and its critics. *Synthese* 2022, 200, 1–33.
13. Jäger, E.; Schmidt, J.; Pfuch, A.; Spange, S.; Beier, O.; Jäger, N.; Jantschner, O.; Daniel, R.; Mitterer, C. Antibacterial Silicon Oxide Thin Films Doped with Zinc and Copper Grown by Atmospheric Pressure Plasma Chemical Vapor Deposition. *Nanomaterials* 2019, 9, 255.
14. Atkins, D.J.; Chau, A.L.; Rosas, J.M.; Chen, Y.-T.; Chan, S.T.; Manuel Urueña, J.; Pitenis, A.A. Silicone Implant Surface Roughness, Friction, and Wear. *Surf. Topogr. Metrol. Prop.* 2023, 11, 014010.